Applications of Three Dimensional Finite Element Method in Orthodontics

ABSTRACT:

systematic manner.

application

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The aim of this paper is to enumerate the various applications of 3D finite element method in Orthodontics. A literature search was done in pub med, embase and cochrane. All articles related to the application of 3D finite element in orthodontics were

collected. The articles were categorized into various sub-

headings based on their use. The various applications of 3D

finite element method in orthodontics have been described in a

Key words: 3D Finite element method, orthodontics,



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INTRODUCTION:

Finite element method (FEM) was developed in 1940 for use in civil and aerospace engineering. Yettram et al introduced this tool in orthodontics in 1972.¹ FEM in orthodontics is used to analyze the structural stress and is considered to be a highly precise technique. An accurate model of tooth and its surrounding structures is offered by this method.

Materials and Method:

A literature search was done in pub med, Embase and Cochrane. All articles related to the application of 3D finite element in orthodontics were collected. The articles were categorized into various

FEM in Maxillary Protraction:

subheadings based on their use.

Dong R et al established a three dimensional finite element model of the craniofacial complex and analysed the force direction of protraction on the temperomandibular joint.² The force applied on the chin was 5N.The angle of force direction was 40* relative to the occlusal plane when the stress and displacement was relatively small.

Indian Journal of Dental Advancements Journal homepage: www. nacd. in Liu c et al analyzed the maxillary growth based on the labiolingual appliance during the maxillary protraction treatment cycle.³ A three dimensional stimulation of labiolingual appliance was performed.

Yanx et al analyzed the bio mechanical effects on the cranio maxillary complex of bone during maxillary protraction.⁴ The direction of forces were 0^* , 10^* , 20^* and 30^* forward and downward relative to the occlusal plane.

The bio mechanical effects of maxillary protraction was also investigated by Chen zx et al with and without maxillary expansion on a model of unilateral cleft lip and palate before and after alveolar bone graft.⁵

FEM and Arch Wire Activation:

Canales et al birth death technique in orthodontic brackets proved to be a bio mechanical stimulation for placement of continuous arch wires.⁶

De Oliveira BF et al established that greater tooth displacement was found in shortened dental arches than in complete dental arches.⁷ An increase in arch perimeter was associated with mandibular lateral expansion.⁸ Inter molar expansion of 1mm increased the arch perimeter by 0.30mm. In sliding mechanics a three dimensional finite element analysis was used by Tominaga et al to simulate en masse anterior tooth retraction.⁹ On the application of retraction force the displacement of maxillary incisor and arch wire deformation were calculated. An x et al investigated the effect of en masse retraction of maxillary teeth and established that excessive retraction can be avoided and intrusion and torque control can be achieved.¹⁰

FEM and Mini -Implants:

Holberg N et al found that when indirect miniimplant anchorage was used, FEM results revealed high loads on dental anchorage.¹¹ Holberg C et al revealed that bio cortical implant anchorage is more favourable biomechanically than mono cortical anchorage.¹²

Ludwig B et al analysed rapid palatal expansion with hybrid Hyrax appliance and stated that it is a suitable device as it delivered a force at the resistance of the nasomaxillary complex through the 2 mini implants. $^{\rm 13}$

Maxillary expansion was attempted in adult patients with fused inter maxillary sutures and was evaluated by Boryor A et al.¹⁴ Mini-implant supported expansion screw of the inter maxillary suture showed a high tensile stress concentration by finite element simulation. An expansion force of 86 N was established when there was a strain measurement on one of the expansion screws.

Neinkemper M investigated primary and secondary displacement of teeth.¹⁵ Controlled tipping and bodily movement were observed as frequent type of movements. Lin TS et al observed a high bone stress adjacent to the mini implants in relation to increased exposure length.¹⁶

Mini-implant deflection and stress distribution was evaluated by Meher AH et al using FEM.¹⁷ Lee et al tried to establish a correlation between the influence of placement angle and the application of orthopedic force.¹⁸ The stability of mini-implants was reduced when the placement angles was less than 60* with various directions of orthopedic forces. The stability of orthodontic mini- implants was estimated using mandibular deformation under clenching.¹⁹

The biomechanical differences between the direct and indirect anchorage and it's effects on the primary stability of mini- implants was analyzed by HolbergC et al.²⁰ An indirect anchorage was chosen to minimize the risk of losing the mini-implant in case of major orthodontic forces.

The relationship between the force direction and movement patterns was analyzed by Kojima Y et al.²¹ The effect of force direction on movement patterns was demonstrated by mechanical simulations.

The bone stress was investigated by Huang YW et al when mini-implants were used for orthodontic anchorage.²² The bone stress was linearly proportional to the force magnitude. The application of force in the forward direction resulted in highest values. Lee et al evaluated stress distribution in Mandibular molar region.²³ Slightly less displacement was appreciated in the angled orthodontic mini- implants(OMIs) than the OMI placed at 90*. The maximum Von Mises stress increased with the inclination of the loading direction.

FEM and Alveolar Bone:

3-D finite element model of maxillary first molars was established by Wang H et al and the stress magnitude and distribution within the Periodontal ligament of maxillary first molars was calculated when loaded with intrusion force.²⁴

FEM and T-Loops:

The commonly analyzed parameter when segmental T-loop was used for canine retraction is ideal moment to force ratio. The load system was significantly affected due to clinical changes in canine position and angulation. The highest moment to force ratio (8.5-9.3) was showed by upright Opus loops and l-loops, when the loops were centred on the canine brackets.

FEM and Trans Palatal Bar and Twin Block:

Transpalatal arch design was used to optimize unilateral molar rotation correction using a finite element method by Geramy A et al.²⁵ An activation of about 0.1 and 1.0 mm produced the same increasing patterns regarding the energy levels.

FEM and Root Resorption:

The initial effects of stress on the periodontal ligament was compared over time in orthodontic external root resorption ,necrosis and TRAP+cell population.²⁶

FEM and Expanders:

Araugio RM et al analysed that less dental tipping was generated when the ideal screw position is slightly above the maxillary first molar center of resistance.²⁷

FEM in Orthognathic Surgery:

The hybrid technique fixation of the Sagittal split ramus osteotomy was evaluated by SatoFR et al for their mechanical characteristics and stress distribution.²⁸

Fem in Individual Tooth Movements:

Van Schepdael et al analyzed and concluded that the differences between analytical and FEM results were small except at the alveolar crest region, but a success in the global behaviour of PDL was observed.²⁹

Vikram NR et al established an increase in cementum thicknesss when the apical stress induced in the periodontal ligament decreased. ³⁰A stress in the cementum and Periodontal ligament occurred as a result of clinical delivery of an orthodontic force.

Lin YL et al found that there was a higher stress level and homogenous stress distribution in individual teeth with posterior cross bite than teeth with normal occlusion.³¹

Geramy A analyzed a method to move palatally erupted lateral incisors labially.³² Equal forces of about 0.15N were applied. An intrusive component could also be added.

FEM in Brackets:

The bracket design had less influence on the torquing moment.³³ An increased torque control capability was exhibited by wider brackets. Holberg C et al attempted to create an anisotropic finite element method model of mandibular bone and orthodontic bracket.³⁴ The results indicated that the risk of enamel fracture depended on the individual debonding procedure.

FEM in Tip Edge Force System:

Zhang Y et al analyzed the distal and extrusive displacement of maxillary first molar under the effect of tip back bend, which could be controlled by the precise control of the degree and position of tip back bend.³⁵

FEM in Soft Tissues:

Chen S et al did a study to get individualized facial three dimensional FE model for prediction of treatment - related morphological change of facial soft tissue. He found an average deviation of 0.47mm and 0.75mm in the soft and hard tissue respectively.³⁶

Conclusion:

FEM has several applications in orthodontics. Since the finite element method can be used innumerable ways to determine stress pattern for hypothetical situations, it's applications in orthodontics is manifold.

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